

# Implementing Compression Models of OA in Mice and Rats

## Organizers

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## Abstract

Rodent models are critical tools for osteoarthritis (OA) and post-traumatic osteoarthritis (PTOA) research. All rodent models of OA are able to initiate joint degradation, but many current models do not reproduce clinically-relevant injury conditions, due to invasive and non-physiologic injury methods. In addition, many of these injury methods cause an injury response due to invasive surgical procedures, complicating studies of the inflammatory response associated with the injury itself. Compression models of OA/PTOA are able to non-invasively induce knee degeneration using externally-applied mechanical loads, closely mimicking injury conditions relevant to humans. The goal of this workshop is to present various compression models of OA/PTOA in mice and rats, and discuss practical/technical considerations of each of these models.

The three speakers in this workshop have considerable expertise developing and using compression models of OA. Dr. Blaine Christiansen will present his work using the anterior cruciate ligament rupture (ACLR) compression model in mice. Dr. Tristan Maerz will present his work translating the ACLR model to rats. Dr. Marjolein van der Meulen will present her work using the cyclic compression loading model in mice. Group discussion will focus on implementation of these models, strengths and limitations of each method, potential sources of variability, and common hurdles encountered with these models.

## Significance and Purpose

There is emerging interest in compression models of OA that can non-invasively induce joint degeneration in mice and rats using externally-applied mechanical loads. These models can be implemented using a variety of methods, each with its own advantages, limitations, and technical considerations. Given the recent development and characterization of these new models, the literature published with these models to date demonstrates expected variability in terms of disease phenotype, severity, and rate of onset. At present, it remains unclear how much of this variability is due to intrinsic biological effects (i.e. strain-, age-, or sex-specific effects) versus implementation of the mechanical loading regimen. The current lack of standardization in the implementation of compression OA models highlights the need for improved standardization and reproducibility. To this end, the primary purpose of this workshop is to *discuss the development and implementation of compression models of OA in mice and rats*, and *present common hurdles encountered with methods*. The goal of this workshop is to provide insight to investigators who are using compression models of OA or are considering these models for their research.

## Educational Need

Compression models are powerful research tools that can provide novel insights into the joint injury response, even at the earliest time points post-injury. However, these loading models often require specialized equipment and custom-made fixtures that are not universally available, and not always consistent between research groups. Therefore, there is a need to educate researchers about key differences between these models, technical challenges associated with their implementation, and the careful selection of an appropriate compression model for a particular research question. There is also a need to define standardization of each model to facilitate greater reproducibility, and multiple aspects of the mechanical loading regimen warrant discussion (e.g. preloading and preconditioning, loading rate, targeting a load vs targeting a displacement, using break detection, etc.).

## Learning Outcomes

After this workshop, attendees will be familiar with multiple compression models that have been used for studies of OA in mice and rats, including previous findings using these models and practical considerations for successful implementation. They will understand the strengths, limitations, and technical challenges associated with each model, and will have the opportunity to discuss these models with established experts who have pioneered the use of compression models in rodents. This workshop will stimulate important discussion regarding model-dependent aspects of the loading regimen that are anticipated to be contributors to model variability and therefore potential targets for standardization.

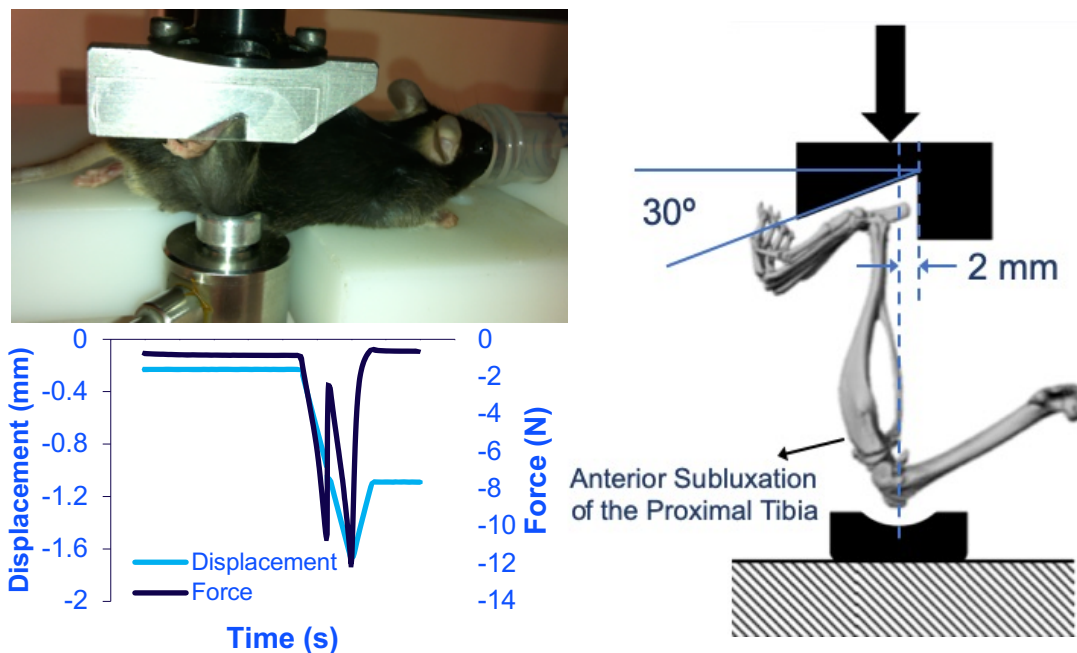
## Compression-Induced ACL Injury in Mice

Blaine A. Christiansen, Ph.D.  
Associate Professor, Department of Orthopaedic Surgery  
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### Introduction:

This injury method uses a single, externally-applied tibial compression overload to non-invasively induce anterior cruciate ligament (ACL) injury in a mouse knee (Christiansen 2012). In this way, this injury model closely recapitulates injury conditions relevant to humans, and allows for analysis of inflammation and other biological processes immediately after injury, since the adaptive response is not confounded by an injection or invasive surgical procedure.

### Description of the Loading Setup:



The lower leg of the mouse is positioned between two loading platens that are aligned vertically in an electromagnetic materials testing machine (ElectroForce 3200, TA Instruments, New Castle, DE). A preload of 1-2 N is applied to hold the lower leg in place. A single compressive load is applied at 1 mm/s to a target force (~12-15 N) or until ACL injury (noted by a release of force and an audible sound), after which the load can be manually stopped.

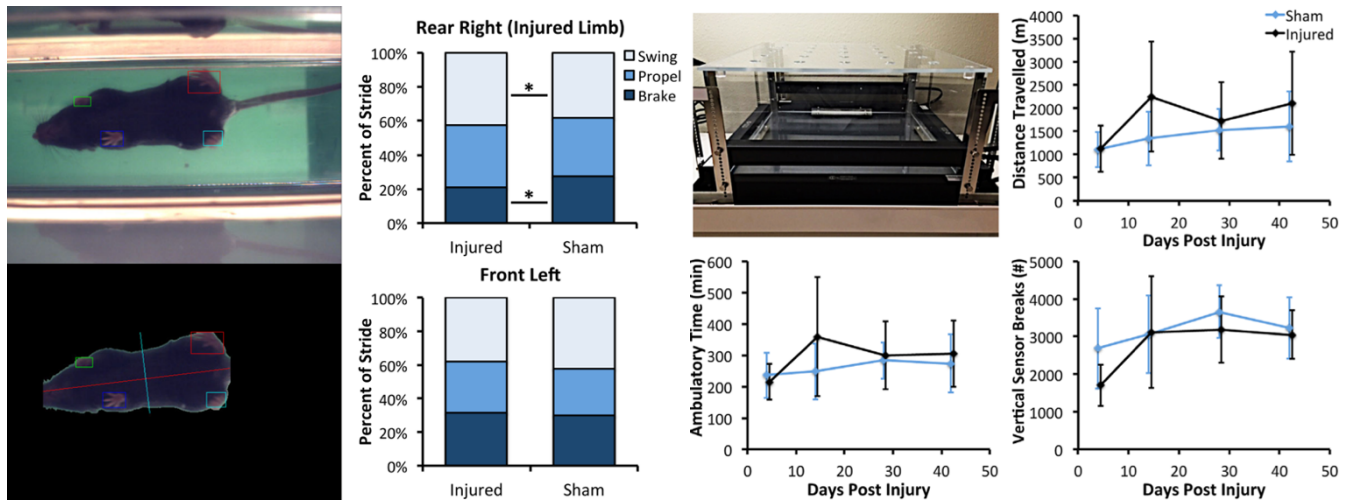
Alternatively, the ACL can be injured by applied a considerably faster load (~200 mm/s) applied to a target displacement (1.7 mm). This type of loading is more likely to induce midsubstance tear of the ACL, rather than avulsion from the distal femur (Lockwood 2014).

For this type of injury, mice are anesthetized with 2-3% isoflurane, and are given a single injection of buprenorphine (0.05 mg/kg SC) at the time of injury. Anesthesia time is typically less than 5 minutes.

### Timeline of OA Progression and Common Observations:

- Following non-invasive ACL injury, joint degeneration progresses to severe OA by 6-8 weeks; the medial side of the joint is more affected than the lateral side
- ACL deficiency causes the articulation of the femur to move to a more posterior position on the proximal tibia; this can lead to dislocation of the posterior horn of the medial meniscus
- Joint inflammation, synovitis, and protease activity are observed primarily during the first 2-3 weeks, peaking around 1-3 days post-injury

- Considerable fibrosis and chondrocyte formation occurs within the first 1-2 weeks; mineralized osteophytes are by 4 weeks post-injury, these will continue to grow and mineralize at later time points
- Osteophytes are commonly observed on the medial side of the distal femur, the posterior-medial proximal tibia, and the medial meniscus
- Epiphyseal trabecular bone loss (~20-40% decrease in BV/TV) occurs during the first 2 weeks post-injury, primarily due to trabecular thinning; this bone loss is partially recovered at later time points
- Thinning of the subchondral bone plate also occurs during the first 2 weeks post-injury; at later time points, this is reversed and subchondral bone plate thickness is increased in injured joints
- No significant differences in overall activity level of mice following injury, though gait analysis indicates a shorter brake phase and longer swing phase in the injured limb (see below)



### **Advantages of this Injury Model:**

- More clinically relevant to human injury than surgical or injection models
- Recapitulates many key features of PTOA in humans
- Once successfully set up, this method is easy to learn with not much expertise required
- Injury is highly reproducible (though faster loading rates are somewhat less reproducible), with a predictable pattern of joint degeneration
- Each injury takes very little time (only takes a few minutes), so can generate high throughput
- Allows for study of inflammation, joint biomechanics, or other processes at early time points, even only a few minutes after injury

### **Limitations of this Injury Model:**

- Creates joint instability; OA progression may be largely driven by mechanical factors
- Severe OA develops within 6-8 weeks, model can't be adjusted to produce a milder injury or slower PTOA progression
- Therapies may be "overpowered" by rapid OA progression, especially at later time points, making it difficult to evaluate long-term therapeutic benefit
- Expensive (and immobile) materials testing system and custom-made attachments usually required

### **Key Findings:**

- No differences in PTOA progression between males and females (Satkunanathan 2014)
- Tibial compression that causes ACL rupture leads to PTOA, while the same load regimen without ACL rupture does not initiate PTOA (Onur 2014)
- Treatment with alendronate following injury inhibits subchondral bone resorption and slows PTOA progression (Khorasani 2015)
- Genetic difference in synovial response at early time points after injury in healer (LGXSM-6) vs. non-healer (LGXSM-33) mouse strains (Duan 2017)
- Differential gene expression following non-invasive ACL injury (Chang 2017)

- Joint range of motion and anterior-posterior joint laxity are increased immediately following injury, but are reduced at later time points, correlating with chondro/osteophyte formation (Hsia 2017)
- Sclerostin (Sost) slows PTOA progression and reduces MMP2/3 protein levels in the joint following injury (Chang 2018)
- MRL/MpJ mice are protected from articular cartilage degeneration following ACL injury, and had reduced expression of inflammatory cytokines and catabolic enzymes (Sebastian 2018)
- Comprehensive analysis of joint inflammation after ACL injury, describing distinct phases of PTOA development, involved tissues/cells, and early molecular changes (Gilbert 2018)
- ACL injury induces metabolomic changes, but inhibition of primary response gene activation with a Cdk9 inhibitor can largely prevent these metabolic changes (Haudenschild 2019)
- Hindlimb unloading following joint injury reduces early protease activity and inhibits osteophyte formation and PTOA progression during subsequent reloading (Hsia, Poster #0600)

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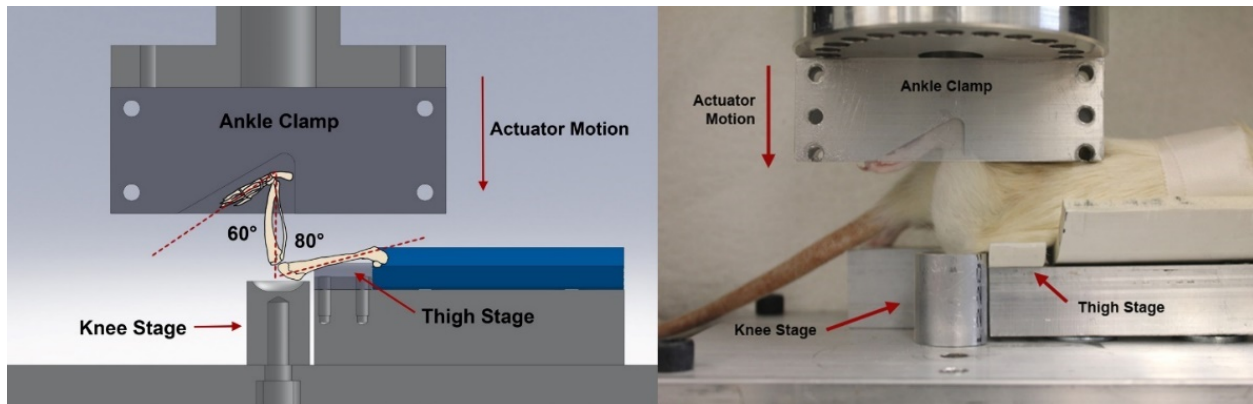
## Compression-Induced ACL Injury in Rats

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### Introduction:

Noninvasive induction of a complete ACL injury in rats enables studies relevant to post-traumatic osteoarthritis (PTOA), acute intra-articular inflammation, and traumatic tissue responses in ligaments, articular cartilage, and subchondral bone. The method in rats is adapted from a similar procedure in mice, described by Christiansen et al (2012). Due to its larger skeletal size, the rat has some unique advantages in both the types of studies (e.g. joint injections requiring volumes larger than 10-15  $\mu$ L) and types of assessments (e.g. articular cartilage imaging), as compared to similar studies in mice.

### Fixtures, Positioning, Anesthesia & Analgesia:



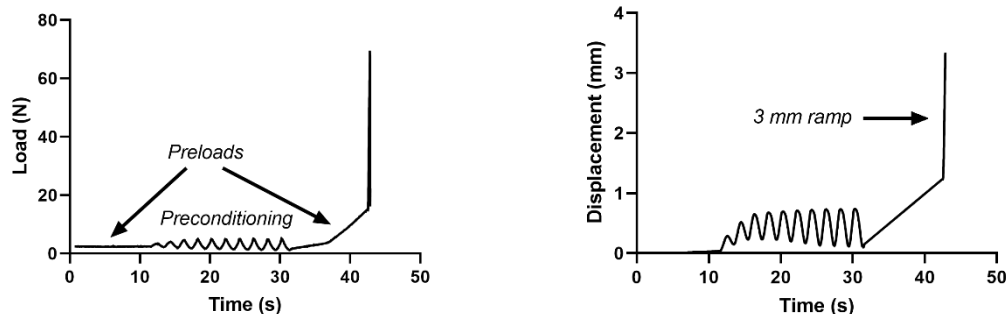
### Considerations

- Appropriately-sized knee stage that restricts medial-lateral motion
  - Both “cup” and “trough/channel” shapes known to work
- Elevation of contralateral limb to height of ipsilateral is important. Pelvic rotation induces ipsilateral femoral internal/external rotation.
- Completely-constrained ankle fixture facilitates injurious motion at the knee
- Quadriceps tendon injury can be avoided/mitigated with padding and/or rounding of edges
- Improper positioning and/or low loading speed may induce dislocation of distal femoral physis

### Anesthesia & Analgesia

- Rats can be anesthetized with ketamine/xylazine or, preferably, with 2-2.5% inhaled isoflurane.
- Post-injury analgesia: 5 mg/kg SC Carprofen and/or 0.05 mg/kg SC buprenorphine.
- Total anesthesia time is 3-5 mins with an additional ~5 mins of recovery monitoring.

### Loading Sequence and Parameters:



### Loading Sequence (as described by Maerz et al Ann Biomed Eng (2015))

- 3N Preload for 10s
- 10x Preconditioning cycles 1N – 5N (0.5 Hz)

- 1 - 15N Preload Ramp (0.1 mm/s)
- Failure ramp: 3 mm downward displacement (8 mm/s)

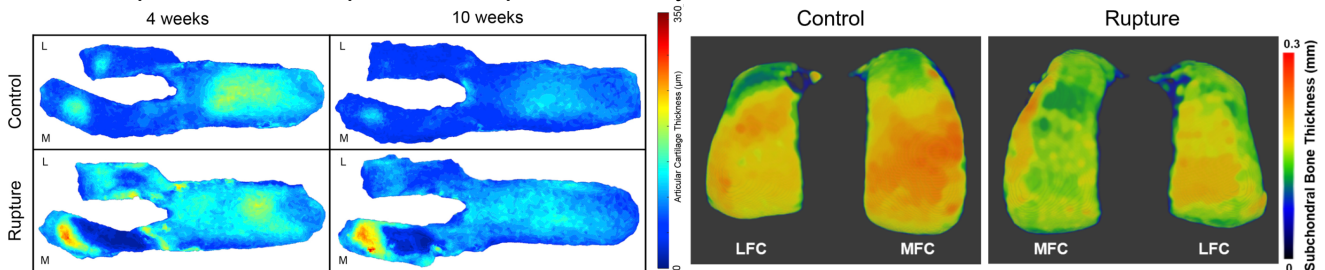
Failure Statistics (200 – 200g Lewis rat):

- Failure Load: 60 – 70 N
- Failure Displacement: 2.2 – 2.5 mm
- Stiffness: 40 – 50 N/mm

\*\*\* Variations of rat ACL rupture models have been described by Ramme et al. (2016, 2018), Brown et al. (2019), and Lepley et al. (2020) \*\*\*

**Timeline of PTOA Progression and Observed Manifestations:**

- General time course of PTOA progression (Maerz 2016, Maerz 2018, Maerz 2016):
  - Early articular cartilage damage observed by 1-2 weeks (surface fibrillation, acute necrosis)
  - Mid-grade OA severity by 4-6 weeks
  - Severe OA by 10 weeks
- Sex differences remain largely uncharacterized
- Medial compartment damage more severe than lateral compartment (below, left) (Maerz 2016)
  - Up to 2x OARSI grade on MFC compared to LFC at 4 weeks
- Synovitis observed as early as 3 days and persisting up to 16 weeks post-injury (Brown 2019, Maerz 2017)
- Acute epiphyseal trabecular bone loss (~20-30% decrease in BV/TV) and subchondral bone thinning (~15-20%) (below, right) is observed within the first 2 weeks. Bone volume deficit of 5-10% observable up to 10 weeks post-injury (Maerz 2016).
- Bony remodeling pattern in epiphyseal trabecular and subchondral bone is complex, compartment-dependent (medial vs lateral), and temporally not unidirectional
  - Importance of compartment-dependent analysis of microCT data



**Advantages of this Injury Model:**

- Completely eliminates potential confounding factors due to surgical injury induction
- Larger skeletal size of rats enables larger joint injection volumes (100-150 µL) and more sensitive analysis of articular cartilage morphology using imaging
- Biomechanical analysis of relative tibiofemoral joint motion demonstrates clinically-relevant injury mechanism similar to human non-contact injury (Maerz 2015)
- *No wound or suture monitoring necessary*
- Highly reproducible procedure with minimal training. No known operator-dependent effects.
- Short procedure time and use of isoflurane for anesthesia enables rapid recovery and minimal anesthesia-dependent effects (i.e. prolonged joint offloading)

**Limitations and Disadvantages:**

- Materials testing system is required for accurate injury induction.
- Chronic destabilization may exacerbate PTOA onset and severity. While ACL reconstruction procedures have been described in the rat, these are unlikely to mitigate and may even exacerbate joint degeneration.
- Higher cost of rats relative to mice
- Uncharacterized but likely significant biomechanical compensation in quadrupeds

- Use of contralateral limb as internal control requires careful consideration and comparison to healthy, age- and sex-matched limbs

### **Key Findings**

- Injury loading induces anterior tibial translation and internal tibial rotation up to the point of ACL failure, at which point rapid external tibial rotation and anterior subluxation occurs (Maerz 2015).
- Rats exhibit less overall osteophyte and chondrocyte formation at similar time points compared to mice.
- Low loading rates (1 mm/s) induce avulsion-type injuries (at femoral side) (Maerz 2015).
- Articular cartilage on medial femoral condyle exhibits zones of severe necrosis and thinning (anterior) and zones of swelling and hypertrophy (posterior) (Maerz 2016).
- Metabolomic characterization of serum demonstrates injury-induced involvement of multiple inflammation and immune-related processes (Maerz 2018).
- Elevated CTX-II and TNF- $\alpha$  levels observed in synovial fluid longitudinally after injury (Brown 2019).
- Reduced bone formation rates and increased bone resorption rates observed by molecular imaging and dynamic histomorphometry acutely after injury (~1-2 weeks) (Maerz 2018, Ramme 2016).
- Progressively-increasing MMP13 expression by articular chondrocytes following injury (Ramme 2016)

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## Load-Induced Joint Injury in Mice

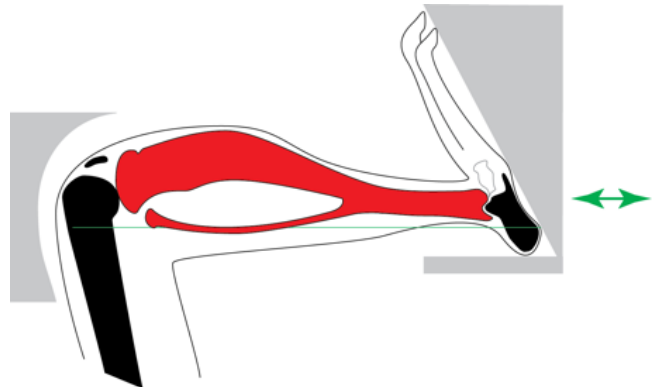
Marjolein C. H. van der Meulen, Ph.D.

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### Introduction:

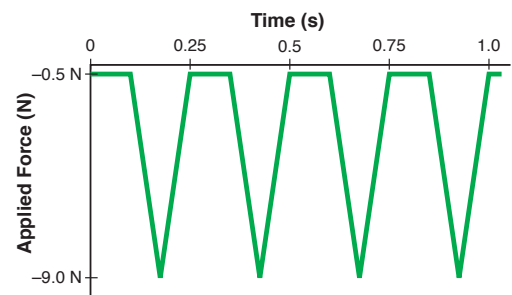
Applying non-invasive compression across the mouse lower limb induces joint damage at the knee with daily and single loading bouts. No surgery is required in this model. All joint structures remain intact, but damage is present. The joint changes differ between the two loading approaches. Cartilage damage is present in both loading regimens; daily loading also induces bone adaptation. This loading approach can also be combined with other methods that induce OA-like changes in the knee.

### Description of the Loading Setup:



The lower leg of the mouse is positioned between two loading platens. We load using a custom-made device with an electromagnetic actuator and load cell with feedback control using LabView. The loading can also be performed using an electromagnetic materials testing machine.

Cyclic compression is applied across the lower limb using a set daily protocol. Loading is performed while the mouse is anesthetized. A small preload of 0.5-1 N is applied to hold the lower leg in place. Our waveform and timing are based on osteogenic loading of the metaphysis. We apply loads at 4 Hz, corresponding to the walking frequency of the mouse at ~4% strain per second. To achieve this loading rate and frequency, we insert a dwell between each load-unload cycle. Loads are determined based on the inducing 1000-1200  $\mu\text{e}$  on the mouse cortex. The load magnitude varies with animal age and strain. Generally loads are in the 7-10N range.



### Timeline of OA Progression and Common Observations:

- With daily in vivo loading cartilage damage is present in both male and female 10-wk and 26-wk-old C57BL/6J mice. The changes are mouse-strain specific. Cartilage damage progresses over time. We have examined 1, 2 and 6 weeks of loading. The joint tissue effects described below are based primarily on male 26-wk-old C57Bl6 mice, unless stated otherwise.
- Bone mass changes are present in the subchondral, epiphyseal and metaphyseal bone. Over time daily loading enhances bone mass at the metaphysis. Changes closer to the joint surface are more variable and may initially decrease at early time points, followed by increased bone mass with time.
- Osteophytes/enthesophytes form on the medial aspect of the joint at the MCL insertion. These structures are cartilaginous after 1 and 2 weeks of loading, and are mineralized at 6 weeks of loading
- Joint fibrosis is present, not classical inflammation. The degree of fibrosis differs substantially across different mouse strains



- Loading induces compression and shear at the joint through AP translation of the tibia and rotation of the femur
- Gait analysis shows no major differences in loaded animals.
- A single bout of loading produces similar effects to daily loading after 1 and 2 weeks.

#### **Advantages of this Injury Model:**

- More clinically relevant to human injury than surgical or injection models
- Recapitulates many key features of OA and PTOA in humans
- The loading is non-invasive, and all joint ligaments remain intact
- Once successfully set up, this method is easy to learn with not much expertise required
- Altering the load magnitude modulates the amount of joint damage generated
- OA development is induced with loading that creates consistent and repeatable joint kinematics
- Implementation can be with small handheld device and laptop computer; however, displacement cannot be measured

#### **Limitations of this Injury Model:**

- OA progression is more rapid than surgical models such as destabilization of the medial meniscus or ACL transection
- Degree of knee flexion may influence joint damage
- Fibrosis is mouse strain-specific, and when severe may produce joint stiffness and likely alters joint loading

#### **Key Findings:**

- Cartilage and joint damage was similar in 10-week and 26-week old C57BL/6 male mice
- Treatment with alendronate during loading exacerbates or protects from joint injury in a mouse-strain specific fashion (Adebayo, et al., 2017)
- Load-induced damage is not additive in mice with spontaneous proteoglycan loss resulting from a mutation in collagen XI (Holyoak, et al., 2018)
- Severe obesity increased load-induced cartilage damage (Guss, et al., 2019)
- The gut microbiome may influence cartilage pathology (Guss, et al., 2019)
- Low magnitude loading can be beneficial and inhibit damage developed in response to surgically-induced damage following destabilization of the medial meniscus (Holyoak, et al., 2019)
- Increased subchondral bone mass and stiffness modulate cartilage damage

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Application of Model:

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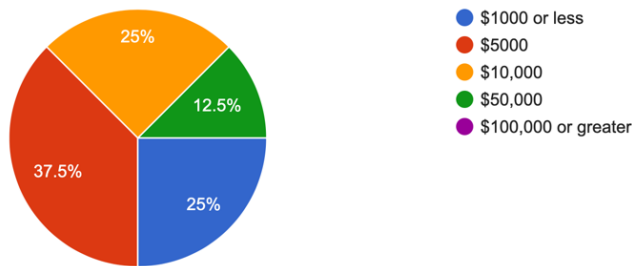
Christiansen BA, Guilak F, Lockwood KA, Olson SA, Pitsillides AA, Sandell LJ, Silva MJ, van der Meulen MC, Haudenschild DR. Non-Invasive Mouse Models of Post-Traumatic Osteoarthritis. *Osteoarthritis Cartilage*. 2015;23(10):1627-38. PMID: 26003950.

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**Appendix: Selected Results from the Pre-Workshop Survey by Current Compression Model Users**

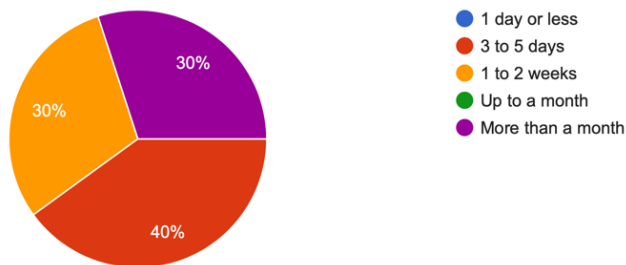
What budget range do you estimate your system for compression model of OA falls within?

8 responses



What time range do you estimate is required to train personnel to reproducibly use the system?

10 responses



*This handout, the full pre-workshop survey results, and other documents from this workshop are available for workshop participants to access at [bit.ly/ORS2020\\_PTOA](http://bit.ly/ORS2020_PTOA) or by scanning the QR code.*

